

Dynamics of Brain Functional Networks and Epileptic Seizures

Kevin Slote¹, Kevin Daley¹, Kelley Smith¹, Charles Epstein², Mukesh Dhamala³, and Igor Belykh¹

¹Department of Mathematics & Statistics and Neuroscience Institute, Georgia State University, Atlanta, GA ²Department of Neurology, Emory University School of Medicine, Atlanta, GA

³Department of Physics and Astronomy, Neuroscience Institute, Center for Behavioral Neuroscience, Georgia State and

Georgia Tech Center for Advanced Brain Imaging, Georgia State University, Atlanta, Georgia

Introduction:

Reconstruction of brain functional networks from iEEG recordings of epileptic episodes: abrupt structural changes and decreased coherence forecast the onset of a seizure

- Epileptic seizures are associated with a state of the brain in which too many neurons are synchronized for the brain to function correctly. Being able to predict the inception of the seizure and notify the person would remove many dangers of its current unpredictability and be a safe temporary solution, while the success rate of brain surgeries and medicine improves.
- There has been a significant success in utilizing the network reconstruction to predict and identifyseizure onset zones using Granger causality¹.
 Researchers have also studied the transitions in network topology acquiring some interesting results¹. Yet, a complete understanding of a global picture of how abnormal synchrony emerges in epilepito brain networks is lacking and requires studies that take into account the interplay between the intrinsic properties of individual neurons and the evolving functional network structures.

Methods:

Network Reconstruction:

Outline: The iEEG data contains voltage readings from electrodes connected directly to the brain, n=120. Since neurons are interconnected, one can analyze these voltage recordings through a statistical measure that gives a numerical value to the strength of connection between different electrodes. Sidingwindow is utilized since the connections are generally not completely connected through all of time. After applying a statistical measure, a threshold sused to drop nodes with weak uncorrelated connections?.

Graph Theoretical Measures:

 Average Betweenness Centrality: The betweenness centrality is the sum of shortest paths that pass through a node V. We average all of these at time t:

$$g = \frac{1}{N} \sum_{v \in G} C_{B(v)}, C_{B(v)} = \sum_{s,t \in V} \frac{\sigma(s,t|v)}{\sigma(s,t)}$$

Average Clustering: The average clustering coefficient is given as:

$$C = \frac{1}{N} \sum_{v \in G} c_v$$

Dynamical Systems Measures:

 Order Parameter: The Kuramoto order parameter was used to measure synchrony in the functional network. The order parameter r (r=1 coherence, r=0 incoherence) is calculated from the IEEEG data using:



References:

¹ Aditiset BM, Epstein CM, Bannala M (2013) Localizing epileptic stizue onests with Ganger causality. *PhysicalReview*. doi:10.1103/1791y RevE&88.030701 9 Varg Z, Tan C, Tanco J, Tohmala M, Luo Z. (2017) A small change in neuronal network: boology can indue exploivve synchronization transition and activity propagation in the entire network. *ScientificReport*. doi:10.1038/s41598.017.00697 SOC

²Papo, D., Zanin, M., & Buldú, J. M. (2014). Reconstructing functional brain networks: have we got the basics right?. Frontier in human neuroscience, 8, 107. doi:10.3389/fnhum.2014.00107



Comparison: The animations show the changes in the network topology over the various episodes for low frequency lowpass filters at 0.25 hz. Compare those to the pictures below that are high pass filters at 50hz



Conclusions:

We have used intracranial electroencephalography (iEEG) recordings of epileptic episodes to reconstruct brain functional networks by applying cross - correlation and calculating graph theoretical measures. By using the graph theoretical measures we have discovered that there were common features to all three episodes even though the episodes were fundamentally different. More specifically, the onset of an epileptic seizure (a severe, generalized seizure in Episode 1, and localized seizures in Episodes 2 and 3) is preceded by a well pronounced episode of decreased coherence and abrupt changes

in functional connectivity. These changes can be used to forecast the onset of a seizure

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> Legend: Red – Epileptic Focus The data consists of 0.25 Hz of iEEG voltage recordings. Sliding window is 4s.